1 Heavy Metal Ion Detection on a Microspot Electrode Using an Optical

- 2 Electrochemical Probe
- 3 Santanu Roy[†], Abhijeet Prasad[†], Rahul Tevatia, Ravi F. Saraf^{*}
- 4 Department of Chemical and Biomolecular Engineering, University of Nebraska,
- 5 Lincoln, NE 68588; [†]Equal contribution; *rsaraf2@unl.edu
- 6

7 **Published in** *Chemelectrochem* **2018**, 5 (3), 429-433

8 The manuscript below may be slightly different from the published MS.

9 Heavy Metal Ion Detection on a Microspot Electrode Using an Optical

10 Electrochemical Probe

- 11 Santanu Roy[†], Abhijeet Prasad[†], Rahul Tevatia, Ravi F. Saraf^{*}
- 12 Department of Chemical and Biomolecular Engineering, University of Nebraska,
- 13 Lincoln, NE 68588; [†]Equal contribution; *rsaraf2@unl.edu

14 Abstract

Electrochemical sensors can be used to create portable, attractive, high-sensitivity devices to detect heavy ions in water at a reasonable cost. A novel method of measuring local redox on an electrode using the differential reflectivity measured on about 6 micron diameter spot using a He/Ne laser beam is described. Field focusing and electrode modification enhances the sensitivity, making the method ideal for miniaturization and multiplexing multiple analytes on a monolith electrode. The method is demonstrated by detecting Pb, Hg, and As ions at ppb and ppt levels.

- 22
- 23 **Keywords:** Heavy metals; electrochemical analysis; electrode size; dielectrophoretic
- 24 effect; water pollution; electro-optics
- 25

26 **1. Introduction**

27 With ever-decreasing sources of water for the growing world population, the search for 28 new sources and the recycling of water have made the issue of heavy metal ion 29 contamination a ubiquitous problem and intensified the need for new detection systems, 30 in terms of sensitivity, specificity, and portability. Toxicity of heavy metal ions is well 31 documented [1-3] with several toxic metals, such as As, Cd, Pb, and Hg, having no 32 known biological function [4]. Heavy metal ions are toxic to reproductive organs of 33 females [5] and males [6], and some are also carcinogens [7]. Concentrations of Pb, 34 Hg, and As in ppb levels a normal human body pose serious health hazards, such as plumbism, hypertension, emphysema, and even cancer with chronic, irreversible 35 damage to organs such as kidneys, skeletal muscles, and soft tissues [8]. Highly 36 sophisticated methods, such as inductively coupled plasma-mass spectroscopy (ICP-37 38 MS) have been developed to measure Cd, Hg, and Pb ions at a sensitivity of 4, 6, and 39 13 ppb, respectively [9]. Optical methods, such as atomic absorption spectroscopy 40 (AAS), X-ray fluorescence spectroscopy (XRF), and inductively coupled plasma-optical 41 emission spectroscopy (ICP-OES), have been developed to measure heavy metal ions 42 at ppb levels [10, 11].

43 Arguably, electrochemical sensors are the most pervasive [11] with innovations in 44 paper-based disposable devices [12] and enhanced sensitivity using nanomaterials [13-45 15] and biopolymers [16]. Apart from the simplicity and expense, electrochemistry is an 46 attractive detection principle because the (redox current) signal is linearly proportional to the analyte concentration. However, the signal (and hence the sensitivity) diminishes as 47 48 the size of the sensor is reduced. The modulation of the refractive index due to the 49 change in ionic interface (i.e., electrical double layer (EDL)) during electrochemical 50 reaction has also been leveraged by static [17] and dynamic [18] interferometry and

51 surface plasmon resonance [19,20]. Here, a simple optical technology based on 52 differential reflectivity is described where the signal increases as the sensing area 53 decreases to naturally decrease the device sensing size to micron levels. The principle 54 of the method and its application for detecting Pb, Hg, and As ions at ppb levels is 55 described.

56 **2. Results and Discussion**

57 The electrochemical reaction (of the redox moiety) was quantitatively probed by 58 measuring the modulation in reflectivity of the sensing electrode due to the change in the interfacial ionic environment around the redox potential (Fig. 1(a)). The 59 electrochemical system consisted of a standard three-electrode arrangement used in 60 61 cyclic voltammetry (CV). The sensor's working electrode (WE) was made of bare Au in 62 contact with a redox ion containing an aqueous solution. The reference electrode (RE) 63 was Ag/AgCl, and Pt wire served as a counter electrode (CE). A potential, E, was 64 applied between the RE and WE; and the current, I, was measured between WE and 65 CE using a potentiostat (Autolab PGSTAT 128N). The WE was patterned with SU8 66 photoresist to expose a circular spot of diameter. d. ranging from 10 to 300 µm. 67 Reflectivity of a He-Ne laser with a beam diameter of about 6 µm was measured from 68 the WE during the CV. The reflectivity was measured as a differential signal by applying additional AC potential of frequency, $\omega = 0.5$ kHz, on the WE. The reflected light 69 70 intensity, R_A , modulated at ω due to ion oscillation caused by AC potential similar to that 71 observed by differential interferometry [18, 21]. From the intensity of the constant 72 reflected light, Ro, measured as a DC signal, differential reflectivity was obtained as, R 73 = R_A/R_0 . A typical signal for R as a function of multiple CV cycles from -0.1 to 0.6 V at a 74 ramp rate of 0.5 V/s for 50 mM of K₄[Fe(CN)₆] showed a highly periodic signal with 75 excellent cycle-to-cycle reproducibility. About 75 scans in 3 minutes were obtained for 76 analysis. For better visualization, magnified view of only a part of the data is shown to 77 underscore the periodicity (Fig. 1(b)). Overlaying all of the cycles and filtering high frequency noise, the average signal, <R>, versus E with robust statistics, was obtained 78 79 (Fig. 1(c)). The error-halo around <R> was the scatter due to cumulative cycle-to-cycle variations. Typically, the noise level at 500 Hz is less than 10⁻⁸Ro. For no ions (i.e., 80 81 blank), <R> is nominally a flat line implying that the signal is absolute.

82 The physical principle of the measurement is considered to relate R to (bulk) ion 83 concentration, [c]. For normal beam, the reflectivity, r by Fresnel's law is, $r = |(N_1-N_2)/$ 84 (N_1+N_2) , where N₁ and N₂ (=n-ik) are complex refractive index of the solution at the 85 interface and metal, respectively. As the ion concentration in the EDL changes due to 86 applied potential, N1 (=n1-ik1) will modulate leading to change in r. Due to small AC potential at ω , the ion concentration at the interface will also oscillate at ω with an 87 88 amplitude of δc_0 . (In principle, ion modulation, δc will decrease as distance from 89 electrode increases. For estimation, with no loss in formulation of the basic concept of 90 the measurement, spatially averaged modulation, δc_{\circ} is considered). As differential 91 refractive index, dn/dc is constant, for small AC potential, $n_1 = N + (dn/dc)\delta c_0 \cos(\omega t)$, 92 where, N is the refractive index at given E (i.e., equilibrium). The higher order oscillation of R_A at 2 ω to 6 ω measured by the lock-in amplifier is >10³-fold smaller than R_A at ω . 93 94 (The higher order effects may occur because of non-linear change in the ion 95 concentration gradient as a function of distance from the electrode/solution interface.)

96 Assuming, the solution to be non-absorbing (i.e., $k_1 = 0$) and for Au, $n^2 << n_1^2$; and 97 because the nonlinearity can be neglected (at 0.1% accuracy), the Fresnel's law for 98 dynamic n_1 can be linerized to yield, |r| (at ω), $R = Q[(dn/dc)\delta c_0]cos\omega t$, where Q =99 $[2n(N^2-k^2)/(N^2+k^2)]$.

100 Next relationship between E and δc_0 is considered to relate the observed R_{max} to [c]. It 101 is well known that, due to slow diffusion kinetics of ions during electrochemical reaction, 102 there is a significant deviation from equilibrium of the ion concentration profile at the 103 interface over a few microns [22]. As a result, the charge in the EDL significantly 104 deviates from neutrality leading to insufficient screening causing a deeper penetration of 105 the electric field emanating from the electrode. This maximization of oscillation of ion 106 amplitude close to redox potentials due to the AC field is consistent with independent 107 (and explicit) observation by differential interferometry [18,21]. Therefore, the reflectivity 108 due to oxidation and reduction peaks at ^oR_{max} and ^rR_{max}, respectively (Fig. 1(c)). At E far 109 from the redox potential, δc_0 is small leading to the small baseline (Fig. 1(c)). 110 Furthermore, as ion diffusion is significantly slower than electron transport in the 111 electrode, EDL discharge is linearly proportional to redox current which in turn is linearly 112 proportional to bulk ion concentration, [c]. Thus, δc_0 is linearly proportional [c]. Thus, 113 after baseline subtraction, at the redox, $R_{max} = PQ[c]$, where P is a calibration constant that will depend on the dynamic properties of the target ions, such as diffusion constant 114 115 and electrophoretic mobility that determines δc_{0} .

By scanning the laser beam and measuring R_{max} , local binding on a monolith electrode can be mapped. If the electrode were to be fabricated as a microarray of a local surface modification, multianalyte detection can be obtained. From known P, the target [c] can be quantified. Importantly, as the polarizability of the ion will change significantly due to its charge state of the ion, a large modulation in n₁ is expected, leading to high responsivity; while k₁ is nominally constant (as change in absorption at 633 nm is not large).

123 A typical <R> versus E for 50 mM showed a large variation in ^{o/r}R_{max} as a function of the 124 patterned spot size, d. As shown by differential interferometry [21], the signal increased as d decreased due to field focusing (i.e., dielectrophoresis) (Fig. 2(a)). The signal was 125 126 further enhanced as the thickness of the photoresist increased from 500 to 1200 nm (compare d = 50 µm for 500 and 1200 nm thickness in Fig. 2(a)). Conventional CV (not 127 128 shown) indicated, as expected, the opposite effect where the peak oxidation current 129 decreased from 50 µA to 20 µA as the size of the spot decreased from 300 µm to 50 µm 130 due to a smaller electrode surface area. A systematic change in d showed the classic 131 field focusing effect where the current density scales as 1/d (Fig. 2(b), inset) [23]. 132 Because, the laser beam diameter was fixed, R_{max} corresponded to the current density 133 rather than the total current [21]. The linear fit for 1/d versus R_{max} was excellent with a 134 small intercept. The intercept of 0.46 corresponds to (limiting) signal for a large planar 135 electrode. Thus, for a spot size of 50 µm and a thickness of 1200 nm, the enhancement 136 due to field focusing relative to a large electrode was ~ 13-fold. For a larger thickness 137 (i.e., 1200 nm in Fig. 2(b)), the signal began to decrease at a smaller d because of the 138 incomplete etching during development of SU8 and the limitations of the lithography 139 process (i.e., dishing effect). For a fixed [c] of 20 ppb, a similar size effect as [Fe(CN)₆]⁴⁻ ^{/3-} is observed with a robust signal for Pb, Hg, and As for d = 50 µm. (Fig 2(c), data only 140

from the oxidation peak is shown). The signal is nominally enhanced by \sim 5-fold as the spot size is reduced from 300 to 50 µm at fixed thickness of 1200 nm.

143 The dielectrophoretic effect was leveraged to measure heavy metal ions (Fig. 3). The 144 three ions tested were As (in As₂O₃), Hg (in HgCl₂), and Pb (in PbCl₂). The calibration 145 curve for all the ions studied is highly linear with fitness of >0.95. The sensitivity to 146 detect Pb ion is significantly enhanced by 3-folds by modifying the Au surface with adsorbed poly(styrene sulfonate) (PSS) (Fig. 3(a)). A robust peak is obtained at 50 ppt 147 148 (Fig. 3(a), inset). The peak for a (baseline corrected) R_{max} of 0.17x10⁻⁴ is difficult to 149 discern, leading to estimated limit of detection (LOD) of ~15 ppt. At ppb levels, the 150 sensitivity of As ion in ppb levels is 1.5 levels lower than Pb on bare Au (Fig. 3(b)). By 151 modifying the Au electrode with PSS and imbedding [Ru(NH₃)₆]³⁺ ions using 32 cycle of 152 CV ranging from -0.5 to 1.2 V, similar to a method described earlier [24], a robust peak 153 is obtained at 1 ppt (Fig. 3(b), inset). Peak below 1 ppt is difficult to discern, leading to 154 LOD of ~1 ppt. Sensitivity to detect Hg ion on bare Au was about 1.5 fold higher than Pb 155 ion at ppb levels (Fig. 3(c)). By imbedding [Fe(CN)₆]⁴⁻ ions on modified Au with PSS and 156 poly(allylamine hydrochloride) PAH layers using the method described earlier [24], a robust peak is obtained at 1 ppt (Fig. 3(c), inset). For Hg, LOD was ~0.5 ppt 157 158 corresponding to R_{max} of ~0.068x10⁻⁴ (close to 1 ppt). All the ion detection was 159 performed at d = 50 μ m and resist thickness of 1200 nm. As indicated for Fig. 1(c), the 160 signal with no ions (i.e., blank) for each modified electrode in the insets of Fig. 3 was 161 zero indicating that R_{max} is an absolute measurement. The mechanism of the imbedded 162 redox ion as described earlier [24], is to function as electron mediator to enhance the 163 redox signal and thereby improve sensitivity. The error bar is calculated from the 164 magnitude of the error halo at R_{max} . As the magnitude of the signal reduces, the width of 165 the error halo also nominally reduces, however the relative error at low [c] is high as 166 shown in the semilog plot (Fig. 3(d)). To demonstrate the guality of the signal averaged 167 over 75 cycles, the inset of Fig. 3(a) to 3(c) shows the raw R with an error halo at the 168 lowest [c] for each ion with no baseline correction. The potentials for R_{max} are consistent 169 with the formal potentials of redox for As, Hg, and Pb ions which are at 320, 380, and 170 280 mV, respectively. Permissible safe levels of As, Hg, and Pb in drinking water set by 171 the United States Environmental Protection Agency are 10, 10, and 15 ppb, 172 respectively. Thus, the low LOD and strong signal at ppb levels in water demonstrates 173 the feasibility of this approach to measuring the toxicity of heavy metal ions in water. 174 Importantly, as multiple redox reactions can be measured on a monolith electrode, by 175 locally modifying the electrodes, it will potentially be possible detect complex mixtures of 176 heavy ions. The reasonableness of the signal (in Fig. 3) is inferred by estimating the ion 177 modulation for measured R. To first order, the dn/dc will primarily be due to the anion 178 owing to its (much) higher polarizability than the cation. Thus, for the chloride salts used 179 in the study, dn/dc ~10⁻¹/M for Hg and Pb salts (based on NaCl). At equilibrium, N \approx 1.4 180 (the ions will raise the interfacial refractive index of water by $\sim 10\%$). For Au (n = 0.18 181 and k = 3.07 at 633 nm) electrode, far from redox, R ~ 0.5x10⁻⁵ leads to $\delta c_0 \sim 2.5$ mM. 182 For 500 ppb solution, R ~10⁻⁴ at redox corresponds to δc_0 of ~50 mM. Although the rise in concentration due to AC potential seems high, for [c] of 500 ppb (i.e., $\sim 2 \mu$ M), the 183 184 enhancement of [CI]⁻ in EDL(at equilibrium) at 200 to 300 mV electrode potential would be in 10⁰ to 10² mM range from classical Poisson-Boltzmann distribution theory. Thus, 185 186 the rough estimation of δc_0 is reasonable within an order of magnitude. Furthermore,

- 187 consistent with the observation, for polyelectrolyte modified electrode n will increase
- and k will be lowered causing an increase of $[2n(N^2-k^2)/(N^2+k^2)]$ to make the electrode
- 189 more sensitive.
- 190

191 3. Conclusions

192 In summary, the differential reflectivity method to measure current density is described 193 where the signal enhances significantly due to field focusing effects and electrode 194 modification. The signal is absolute. Limit of detection of 1 ppt is demonstrated for Hg and As ions, and 50 ppt for Pb ions. The calibration curve for all the three ions was 195 196 highly linear over [c] ranging over five orders of magnitude. Furthermore, as the method 197 measures local redox, potentially, multiple analytes on a monolith electrode can be detected by, for example, locally modifying the electrode surface with different 198 199 polyelectrolytes and redox ions to develop a quantitative "artificial nose" to profile heavy 200 metal ions.

- 201
- 202

203 References

[1] M. Jaishankar, T. Tseten, N. Anbalagan, B.B. Mathew, K.N. Beeregowda, Toxicity,
mechanism and health effects of some heavy metals, Interdiscip. Toxicol. 7 (2014) 6072.

[2] X. Wu, S.J. Cobbina, G. Mao, H. Xu, Z. Zhang, L. Yang, A review of toxicity and
mechanisms of individual and mixtures of heavy metals in the environment, Environ.
Sci. Pollut. Res. Int. 23 (2016) 8244-8259.

- 210 [3] H. Kozlowski, P. Kolkowska, J. Watly, K. Krzywoszynska, S. Potocki, General 211 aspects of metal toxicity, Curr. Med. Chem. 21 (2014) 3721-3740.
- [4] P.B. Tchounwou, C.G. Yedjou, A.K. Patlolla, D.J. Sutton, Heavy metal toxicity andthe environment, EXS. 101 (2012) 133-164.
- 214 [5] P. Rzymski, K. Tomczyk, P. Rzymski, B. Poniedzialek, T. Opala, M. Wilczak, Impact
- of heavy metals on the female reproductive system, Ann. Agric. Environ. Med. 22 (2015) 259-264.
- [6] J.J. Wirth, R.S. Mijal, Adverse effects of low level heavy metal exposure on male
 reproductive function, Syst. Biol. Reprod. Med. 56 (2010) 147-167.
- 219 [7] P. Koedrith, H. Kim, J.I. Weon, Y.R. Seo, Toxicogenomic approaches for
- 220 understanding molecular mechanisms of heavy metal mutagenicity and carcinogenicity,
- 221 Int. J. Hyg. Environ. Health. 216 (2013) 587-598.
- [8] H. Schroeder, D. Darrow, Relation of trace metals to human health, Bost Coll
 Environ Aff Law Rev. 2 (1972) 222–236.

- [9] H. Wang, Z. Wu, B. Chen, M. He, B. Hu, Chip-based array magnetic solid phase
 microextraction on-line coupled with inductively coupled plasma mass spectrometry for
- the determination of trace heavy metals in cells, Analyst. 140 (2015) 5619-5626.
- [10] B.K. Bansod, T. Kumar, R. Thakur, S. Rana, I. Singh, A review on various
 electrochemical techniques for heavy metal ions detection with different sensing
 platforms, Biosensors and Bioelectronics. 94 (2017) 443-455.
- [11] L. Pujol, D. Evrard, K. Groenen-Serrano, M. Freyssinier, A. Ruffien-Cizsak, P. Gros,
 Electrochemical sensors and devices for heavy metals assay in water: the French
 groups' contribution, Front. Chem. 2 (2014) 19.
- [12] N.A. Meredith, C. Quinn, D.M. Cate, T.H. Reilly 3rd, J. Volckens, C.S. Henry,
 Paper-based analytical devices for environmental analysis, Analyst. 141 (2016) 18741887.
- 236 [13] P. Ramnani, N.M. Saucedo, A. Mulchandani, Carbon nanomaterial-based 237 electrochemical biosensors for label-free sensing of environmental pollutants,
- 238 Chemosphere. 143 (2016) 85-98.
- [14] M. Govindhan, B. Adhikari, A. Chen, Nanomaterials-based electrochemical
 detection of chemical contaminants, RSC Adv. 4 (2014) 63741-63760.
- [15] M. Li, H. Gou, I. Al-Ogaidi, N. Wu, Nanostructured Sensors for Detection of Heavy
 Metals: A Review, ACS Sustainable Chem. Eng. 1 (2013) 713-723.
- [16] Y. Zhou, L. Tang, G. Zeng, C. Zhang, Y. Zhang, X. Xie, Current progress in
 biosensors for heavy metal ions based on DNAzymes/DNA molecules functionalized
- nanostructures: A review, Sensors and Actuators B: Chemical. 223 (2016) 280-294.
- [17] Q. Li, H.S. White, Interferometric Measurement of Depletion Layer Structure and
 Voltammetric Data in Concentrated Organic Redox Solutions, Anal. Chem. 67 (1995)
 561-569.
- [18] G. Singh, D. Moore, R.F. Saraf, Localized Electrochemistry on a 10 um Spot on a
 Monolith Large Electrode: An Avenue for Electrochemical Microarray Analysis, Anal.
 Chem. 81 (2009) 6055-6060.
- [19] D.G. Hanken, R.M. Corn, Electric Fields and Interference Effects inside
 Noncentrosymmetric Multilayer Films at Electrode Surfaces from Electrochemically
 Modulated Surface Plasmon Resonance Experiments, Anal. Chem., 69 (1997) 36653673.
- [20] X. Shan, U. Patel, S. Wang, R. Iglesias, N. Tao, Imaging Local Electrochemical
 Current via Surface Plasmaon Resonance, Science, 327 (2010) 1363-1366.

- [21] S.W. Lee, J. Lopez, R.F. Saraf, Direct mapping of local redox current density on a
 monolith electrode by laser scanning, Biosens. Bioelectron. 47 (2013) 408-414.
- [22] R.G. Compton, C.E. Banks, Understanding Voltammetry, second ed., ImperialCollege Press, London, 2011.
- [23] D.W. Arrigan, Nanoelectrodes, nanoelectrode arrays and their applications,Analyst. 129 (2004) 1157-1165.
- [24] S.W. Lee, J. Lopez, R.F. Saraf, Fabrication and Properties of Redox Ion Doped
 Few Monolayer Thick Polyelectrolyte Film for Electrochemical Biosensors at High
 Sensitivity and Specificity, Electroanalysis. 25 (2013) 1557-1566.





Figure 2. (a) Redox signal for 50 mM K₄[Fe(CN)₆] as a function of resist thickness (nm) and the electrode diameter (\Box m). (b) R_{max} as a function of d for resist thickness of 1200 and 500 nm. Inset: Linear correlation of R_{max} versus 1/d for resist thickness of 500 nm. (c) The variation in R_{max} for heavy metal ions with d.

322





379 Figure 3. The calibration curve of heavy metal ions with linear relation between R_{max} 380 and [c] (d= 50 and resist thickness = 1200 nm). (a) Pb on bare Au (ppb levels) and PSS 381 modified Au (ppt levels). The responsivity (i.e., slopes) are 0.00125 and 0.00350 for the 382 ppb and ppt levels, respectively. The inset shows raw data for 50 ppt Pb. (b) As on bare Au (ppb levels) and PSS modified Au with imbedded [Ru(NH₃)₆]³⁺ ions (ppt levels). The 383 384 responsivity are 0.00081 and 0.00486 for the ppb and ppt levels, respectively. The inset 385 shows raw data for 1 ppt As. (c) Hg on bare Au microelectrode (ppb levels) and PSS and PAH modified with [Fe(CN)₆]⁴⁻ ions (ppt levels). The responsivity are 0.00178 and 386 387 0.00245 for the ppb and ppt levels, respectively. The inset shows raw data for 1 ppt Hg. 388 The blank in the insets is R to the corresponding modified electrode in distill water. (d) 389 Semilog plot of calibration curves to show relative error.